









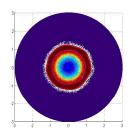


# Some equations from mathematical biology

#### **Benoît Perthame**









- The status of physics his written in the names of equations
- What are the fundamental principle of biology?



- The status of physics his written in the names of equations
- What are the fundamental principle of biology?
- Is mathematics the good language for life sciences?



- The status of physics his written in the names of equations
- What are the fundamental principle of biology?

"Science is a differential equation" (Alan Turing)



- The status of physics his written in the names of equations
- Newton's fundamental principle of dynamics

$$\begin{cases} \frac{d}{dt}X(t) = V(t) \\ \frac{d}{dt}V(t) = F(X(t), V(t)) \end{cases}$$





- The status of physics his written in the names of equations
- Fluid flows (Navier-Stokes eq., 1823-1845)

$$\left\{ \begin{array}{l} \frac{\partial}{\partial t} u + u.\nabla u + \nabla p = \nu \Delta u, \\ \operatorname{div} u = 0 \end{array} \right.$$

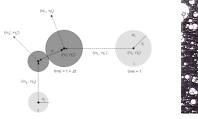


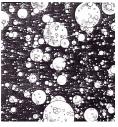






# L. Boltzmann - A gas is the result of collisions between molecules (1872)





 $f(x, \xi, t) = \text{density of molecules with velocity } \xi \in V = \mathbb{R}^3$ 

$$\underbrace{\frac{\partial}{\partial t} f(x, \xi, t) + \xi. \nabla_{x} f}_{\text{Transport with velocity } \xi} = \underbrace{Q(f, f)}_{\text{Binary collisions}}$$



#### PARTICLE SCALE

$$\begin{cases} \frac{d}{dt}X_i(t) = V_i(t), & 1 \leq i \leq N, \\ \frac{d}{dt}V_i(t) = F(X(t), V(t)) \end{cases}$$

## KINETIC/DILUTE GAS $N \to \infty$

$$\frac{\partial}{\partial t} f(x, \xi, t) + \xi . \nabla_x f = \frac{1}{\kappa} \underbrace{Q(f, f)}_{\text{Binary collisions}}$$

# MACROSCOPIC/FLUID $\kappa \to 0$

$$\begin{cases} \frac{\partial}{\partial t} u + u \cdot \nabla u + \nabla p = \nu \Delta u, \\ \operatorname{div} u = 0 \end{cases}$$



■ The status of physics his written in the names of equations

$$-\Delta u = f \qquad \qquad \text{(Laplace/Poisson)}$$
 
$$\frac{\partial^2 u}{\partial t^2} - \Delta u = 0 = \Box u \qquad \qquad \text{(D'Alembert)}$$
 
$$\frac{\partial u}{\partial t} - \Delta u = 0 \qquad \qquad \text{(Fourier)}$$
 
$$\left\{ \begin{array}{l} \operatorname{div} E = 0, & \operatorname{curl} E = -\frac{\partial B}{\partial t} \\ \operatorname{div} B = 0, & \operatorname{curl} B = -\frac{1}{c^2} \frac{\partial E}{\partial t} \end{array} \right. \qquad \text{(Maxwell)}$$
 
$$i \frac{\partial u}{\partial t} - \Delta u = 0 \qquad \qquad \text{(Schrödinger)}$$

# Names of PDE of physics



	Euler	Lagran	ige Liouville	Boussinesq		
	Hamilton-Jacobi		Bellman	Kirchhoff		
	Allen-Cahn Ca Ginzburg-Landau Thomas-Fermi		nn-Hilliard	Vlasov	Landau	
			Gross-Pitaevs			
			Einstein			
	Dirac Airy		Kolmogorov	Fokker-Planck		
	Monge-Am	oère Kor	teweg de Vries	Camassa-Holme		
	Maxwel	l-Stefan	Kuramoto-Shiva	ashinsky	Choquard	
	Burgers	Lorentz	Saint-Venant	Benjamir	n-Ono	
	KPP	KPZ	Zhakarov	Born-I	nfeld = >	) ५ (२



# And in biology?



## And in biology?

$$\begin{cases} \frac{dS(t)}{dt} = aS(t) - bS(t)P(t), \\ \frac{dP(t)}{dt} = -cP(t) + bS(t)P(t), \end{cases}$$
 (Lotka-Volterra)

Became a generic name for a class of equations in ecology

#### Lotka-Volterra



- $\mathbf{x}$  = phenotypical trait (size, type of nutrient,...)
- n(x, t) =number of individuals of type x
- S(t) =environment (nutrient)

#### Lotka-Volterra



- $\mathbf{x}$  = phenotypical trait (size, type of nutrient,...)
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- S(t) = environment (nutrient)

#### change in number

mutations

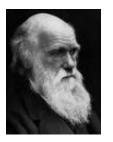
$$\frac{\partial n(x,t)}{\partial t} = \underbrace{R(x,S(t))}_{\text{growth/death rate}} n(x,t) + \underbrace{\mu \int b(y,S(t))M(y\rightarrow x)n(y,t)dy}_{\text{growth/death rate}}$$

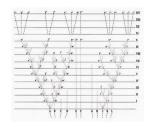
$$S(t) = S([n(t)])$$
  $S(t) = \frac{S_0}{1 + \int n(x, t) dx}$ 

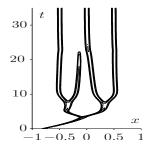
This expresses selection by competition with finite resources

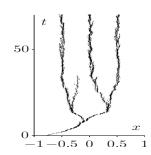
## Lotka-Volterra











There is a small parameter for mutations



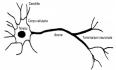
## **Neuroscience**

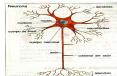


The electrically active cells are described by

- **action potential** v(t)
- ionic chanels  $g_i(t)$







#### Neuroscience



The electrically active cells are described by

- **action potential** v(t)
- ionic chanels  $g_i(t)$
- Hodgkin-Huxley
- Morris-Lecar
- Mitchell-Schaeffer
- FitzHugh-Nagumo

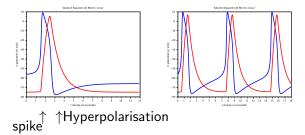
$$\begin{cases} \frac{dv(t)}{dt} = \sum_{i} g_i(t) (V_i - v(t)) + I(t) \\ \frac{dg_i(t)}{dt} = \frac{G_i(v(t)) - g_i(t)}{\tau_i}, \end{cases}$$

## **Neuroscience**



The electrically active cells are described by

- **action potential** v(t)
- ionic chanels  $g_i(t)$





The Leaky Integrate & Fire model is simpler

$$dv(t) = (-v(t) + I(t))dt + \sigma dW(t), \qquad v(t) < V_{\mathrm{Firing}}$$
  $v(t_{-}) = V_{\mathrm{Firing}} \implies v(t_{+}) = V_{\mathrm{Reset}}$   $0 < V_{R} < V_{F}$ 

- I(t) input current
- Noise or not

- Much simpler that Hodgkin-Huxley/Morris-Lecar models
- The idea was introduced by L. Lapicque (1907)

# A short break



## Brother of Charles Lapicque









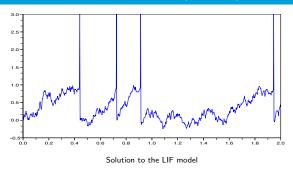
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- N. Brunel and V. Hakim, R. Brette, W. Gerstner and W. Kistler, Omurtag, Knight and Sirovich, Cai and Tao...
- Fit to measurements
- Use more realistic dynamics in place of -v



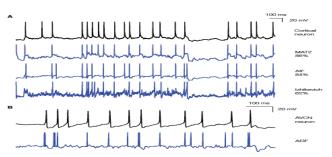


FIGURE 4 | Fitting spiking models to electrophysiological recordings. (A) The response of a cortical pyramidal cell to a fluctuating current (from the INICE competition) is fitted to versious models; MAT (Ecohyspikin) et al., 2000; Apptive integrate-and-fire, and briskevich (2003). Performance on the training data is indicated on the right as the gamma factor (close to the proportion of predicted spikes), relative to the intrinsic gamma factor of the neuron (i.e., proportion of colors to the proportion of the response of the proportion of the colors of the proportion of the colors of the proportion of the colors of the color

From C. Rossant et al, Frontiers in Neuroscience (2011)

#### **Noisy LIF networks**



It is now possible to write a system of N interacting neurons,

- For  $1 \le j \le N$
- with  $t_j^k$  the spiking times :  $v_j(t_j^{k-}) = V_F$
- $v_j(t_j^{k+}) = V_R$

$$\frac{d}{dt}v_i(t) = -v_i(t) + \underbrace{\frac{\beta}{N} \sum_{j=1}^{N} \sum_{k} \delta(t - t_j^k)}_{\text{current generated by spikes}} + \sigma dW_i(t), \qquad v_i(t) < V_F$$

## **Noisy LIF networks**



See Delarue, Inglis, Rubenthaler, Tanre, Tallay, Locherbach, Lucon:

For assemblies, the mean field limit yields a current I = bN(t)

$$\begin{cases} \frac{\partial n(v,t)}{\partial t} + \frac{\partial}{\partial v} \left[ \left( -v + bN(t) \right) n(v,t) \right] - a \left( N(t) \right) \frac{\partial^2 n(v,t)}{\partial v^2} = N(t) \, \delta_{V_R}(v), \\ v \leq V_F, \\ n(V_F,t) = 0, \qquad n(-\infty,t) = 0, \end{cases}$$

$$N(t) := -a \left( N(t) \right) \frac{\partial}{\partial v} n(V_F,t) \geq 0, \qquad \text{flux of firing neurons at } V_F$$

#### Constitutive laws

- b = connectivity
- $\blacksquare b > 0$  excitatory neurones
- $\mathbf{b}$  < 0 inhibitory neurones

$$a(N) = a_0 + a_1 N$$

# Noisy LIF networks (blow-up)



Theorem (M. Cáceres, J. Carrillo, BP) [excitatory, blow-up] Assume  $a \ge a_0 > 0$  and b > 0. Then the solution blows-up in finite time in the two cases

- the initial data is concentrated enough around  $v = V_F$  (depending on b)
- initial data is given, b is large enough

#### Surprisingly

- Noise does not help
- value of b does not count

## Noisy LIF with refractory state



**Proof.** For  $\mu = 2 \max(\frac{1}{b}, \frac{V_F}{a_0})$ , define

$$\phi(v) = e^{\mu v}, \qquad M_{\mu}(t) := \int_{-\infty}^{V_F} \phi(v) n(v, t).$$

For smooth solutions, we prove that  $M_{\mu}(t)$  becomes larger than  $e^{\mu V_F}$ 

$$\frac{dM_{\mu}}{dt} = \mu \int_{-\infty}^{V_F} (bN(t) - v + \mu a) \phi(v) p(v, t) - N(t) \phi(V_F) + \frac{N(t)}{\tau} \phi(V_R)$$

$$\geq N(t) \underbrace{\left[b\mu M_{\mu}(t) - \phi(V_F)\right]}_{\geq \mu V_F > 0} + \underbrace{\mu \left[\mu a_0 - V_F\right]}_{\geq \mu V_F > 0} M_{\mu}(t)$$

$$> 0 \text{ is needed only initially}$$

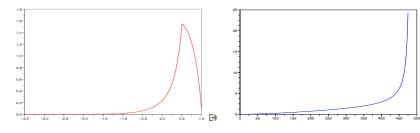
OK for b large enough or  $M_{\mu}(0)$  large enough

To go further : the difficulty : no relation between  $M_{ii}$  and N



# Noisy LIF networks (blow-up)





Excitatory integrate and fire model. Blow-up case. Left p(v, t), Right : N(t)

# Noisy LIF networks (blow-up)



#### Possible interpretation

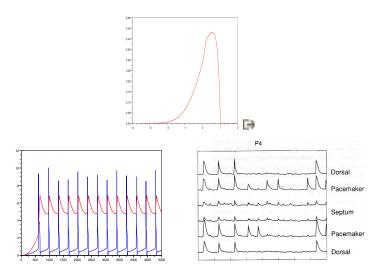
- $lacksquare N(t) 
  ightarrow 
  ho \delta(t-t_{
  m BU})$  and  $t_{
  m BU} > 0$ ,
- partial synchronization

Simplified models : Kuramoto, Carillo-Ha-Kang, Dumont-Henry, Giacomin, Pakdaman



# Spontaneous activity (regularized)





Left: Excitatory integrate & fire with refractory state and random firing threshold Right: Conhaim et al (2011) J. of physiology 589(10) 2529-2541.





#### Paradigm for collective organisation



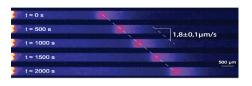


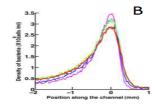


Left : Courtesy S. Seror, B. Holland (Paris-Sud),

Right: Numerical simulation of a mathematical model







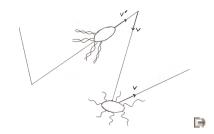
- Adler's famous experiment for *E. Coli* (1966) chemotactic
- Explain this pattern; its asymmetry (experiments Curie institute)

■ How can a model of chemotaxis (Keller-Segel) generate robust trvaeling pulses?



E. Coli is known to move by run and tumble Alt, Dunbar, Othmer, Stevens, Hillen, Schmeiser...





A beautiful example of multiscale motion



- $f(t,x,\xi)$  population density of cells moving with velocity  $\xi$
- c(t,x) the chemoattractant concentration

$$\frac{\partial}{\partial t} f(t, x, \xi) + \underbrace{\xi \cdot \nabla_{x} f}_{\text{run}} = \underbrace{\mathcal{K}[c, S] f}_{\text{tumble}},$$

$$\mathcal{K}[c, S] f = \int_{B} K(c, S; \xi, \xi') f(\xi') d\xi' - \int_{B} K(c, S; \xi', \xi) d\xi' f,$$

$$\kappa[c, S] f = \int_{B} \kappa(c, S; \xi, \xi) f(\xi) d\xi - \int_{B} \kappa(c, S; \xi, \xi) d\xi$$
$$-\Delta c = n(x, t) := \int f(t, x, \xi) d\xi$$

■ Typical is pathwise sensing

$$K(c; \xi, \xi') = K(\partial_t c + \xi' \cdot \nabla_x c)$$



#### Multiscale analysis based on the stiffness

Define the small parameter  $\varepsilon$ 

$$K(c; \xi, \xi') = \mathbf{K}_{\varepsilon} \left( \underbrace{\frac{\partial c}{\partial t} + \xi' \cdot \nabla c}_{D_t c} \right)$$

$$\begin{cases} \frac{\partial}{\partial t} f_{\varepsilon}(t, x, \xi) + \frac{\xi \cdot \nabla_{x} f_{\varepsilon}}{\varepsilon} = \frac{\mathcal{K}[c_{\varepsilon}, f_{\varepsilon}]}{\varepsilon^{2}}, \\ -\Delta c_{\varepsilon}(t, x) = n_{\varepsilon}(t, x) := \int f_{\varepsilon}(t, x, \xi) d\xi. \end{cases}$$



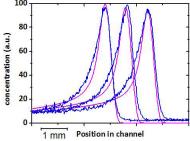
#### Multiscale analysis based on sensing stiffness

Theorem (Diffusion limit)

As  $\varepsilon$  vanishes,  $f_{\varepsilon} \to n(x,t) \mathbb{1}_{\{v \in V\}}$  and

$$\begin{cases} \frac{\partial}{\partial t} n(t, x) - \Delta n(t, x) + \operatorname{div}(nU) = 0 \\ -\Delta c(t, x) = n(t, x) \\ U = \phi(|\nabla c|) |\nabla c| \end{cases}$$

Flux Limited Keller-Segel system





#### **POPULATION SCALE**

$$\begin{cases} \frac{\partial}{\partial t} n(t, x) - \Delta n(t, x) + \operatorname{div}(nU) = 0 \\ -\Delta c(t, x) = n(t, x), \qquad U = \phi(|\nabla c|) |\nabla c| \end{cases}$$

#### KINETIC/INDIVIDUAL SCALE

$$\frac{\partial}{\partial t} f_{\varepsilon}(t, x, \xi) + \frac{\xi \cdot \nabla_{x} f_{\varepsilon}}{\varepsilon} = \frac{\mathcal{K}[c_{\varepsilon}, f_{\varepsilon}]}{\varepsilon^{2}},$$

#### **Bacterial motion**



#### POPULATION SCALE

$$\begin{cases} \frac{\partial}{\partial t} n(t, x) - \Delta n(t, x) + \operatorname{div}(nU) = 0 \\ -\Delta c(t, x) = n(t, x), \qquad U = \phi(|\nabla c|) |\nabla c| \end{cases}$$

#### KINETIC/INDIVIDUAL SCALE

$$\frac{\partial}{\partial t} f_{\varepsilon}(t, x, \xi) + \frac{\xi \cdot \nabla_{x} f_{\varepsilon}}{\varepsilon} = \frac{\mathcal{K}[c_{\varepsilon}, f_{\varepsilon}]}{\varepsilon^{2}},$$

#### **MOLECULAR SCALE**

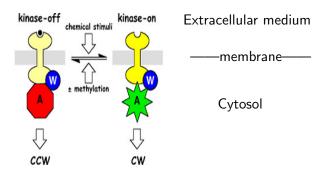
$$\frac{\partial}{\partial t} f_{\varepsilon}(t, x, \xi, y) + \xi \cdot \nabla_{x} f_{\varepsilon} + \frac{1}{\varepsilon} \operatorname{div}_{y} [R_{\varepsilon} f_{\varepsilon}] = \Lambda_{\varepsilon}(y) \int [f_{\varepsilon}(\xi') - f_{\varepsilon}(\xi)] d\xi'$$

# **Biochemical pathways**



#### Can one explain the tumbling rate

$$K(c; \xi, \xi') = \mathbf{K} \left( \frac{\partial c}{\partial t} + \xi' \cdot \nabla c \right)$$
?



# **Biochemical pathways**



# Can one explain the tumbling rate $K(\frac{\partial c}{\partial t} + \xi' . \nabla c)$ ?

Departing from

$$\frac{\partial}{\partial t} f_{\varepsilon}(t, x, \xi, y) + \xi \cdot \nabla_{x} f_{\varepsilon} + \frac{1}{\varepsilon} \operatorname{div}_{y} [R_{\varepsilon} f_{\varepsilon}] = \Lambda_{\varepsilon}(y) \int [f_{\varepsilon}(\xi') - f_{\varepsilon}(\xi)] d\xi'$$

**Theorem** As  $\varepsilon \to 0$ , the limit is

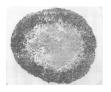
$$f_{\varepsilon}(t,x,\xi,y) \to \bar{f}(t,x,\xi)\delta(y=Y(c))$$

and

$$\begin{split} &\frac{\partial}{\partial t}\bar{f}(t,x,\xi) + \xi \cdot \nabla_x \bar{f} = \\ &= \int \left[ \mathbf{K} \left( \frac{\partial c}{\partial t} \right. + \xi' \cdot \nabla c \right) \bar{f}(\xi') - \mathbf{K} \left( \frac{\partial c}{\partial t} \right. + \xi \cdot \nabla c \right) \bar{f}(\xi) \right] d\xi' \end{split}$$

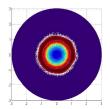


#### Models used for tumor growth











#### **Simplest** model is mechanical only:

n(x,t) = population density of tumor cells at location x, time t, v(x,t) = cell velocity at location x and time t, p(x,t) = pressure in the tissue,

Change in number of cells

$$\frac{\partial n}{\partial t} = \underbrace{-\operatorname{div}(nv)}_{\text{movement of cells}} + division - death$$

Darcy's law for friction (with ECM) dominated flow

$$v = -\nabla p(x, t),$$

Constitutive law (compressible fluid)

$$p(x, t) \equiv \Pi(n) := n^{\gamma}, \quad \gamma > 1$$

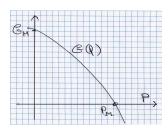




The compressible mechanical model

$$\left\{ \begin{array}{l} \frac{\partial}{\partial t} n + \operatorname{div} \big( n v \big) = n G \big( p(x,t) \big), \qquad x \in \mathbb{R}^d, \ t \geq 0, \\ \\ v = - \nabla p(x,t), \qquad p(x,t) \equiv \Pi(n) := n^\gamma, \quad \gamma > 0. \end{array} \right.$$

Byrne, Drasdo, Chaplain, Joanny-Prost-Jülicher...etc 'homeostatic pressure'





#### The compressible mechanical model

$$\left\{ \begin{array}{l} \frac{\partial}{\partial t} n + \operatorname{div} \big( n v \big) = n G \big( p(x,t) \big), \qquad x \in \mathbb{R}^d, \ t \geq 0, \\ \\ v = - \nabla p(x,t), \qquad p(x,t) \equiv \Pi(n) := n^\gamma, \quad \gamma > 0. \end{array} \right.$$

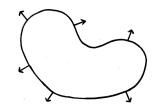
#### Specific properties

$$\blacksquare \frac{\partial}{\partial t} n(t=0) \ge -\frac{C}{t} e^{-\gamma c_G t}$$



Spatial domain  $\Omega(t)$ 

$$v(x,t) = -\nabla p(x,t)$$



Compute the pressure as

$$\begin{cases} -\Delta p = G(p) & x \in \Omega(t), \\ p = 0 & \text{on } \partial \Omega(t). \end{cases}$$

Surface tension may be included ( $\kappa = \text{mean curvature}$ )

$$p(x, t) = \eta \kappa(x, t),$$
 on  $\partial \Omega(t)$ 



$$\begin{cases} \frac{\partial}{\partial t} n_{\gamma} + \operatorname{div}(n_{\gamma} v_{\gamma}) = n_{\gamma} G(p_{\gamma}(x, t)), & x \in \mathbb{R}^{d} \\ v_{\gamma} = -\nabla p_{\gamma}(x, t), & p_{\gamma}(x, t) \equiv \Pi(n_{\gamma}) := n^{\gamma}, \end{cases}$$

Theorem (Hele-Shaw limit) : As  $\gamma \to \infty$ 

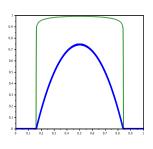
$$n_{\gamma} 
ightharpoonup n_{\infty} \leq 1, \qquad p_{\gamma} 
ightharpoonup p_{\infty} \leq p_{M}$$
 
$$\left\{ egin{array}{l} rac{\partial}{\partial t} n_{\infty} - \operatorname{div}ig(n_{\infty} 
abla p_{\infty}ig) = n_{\infty} Gig(p_{\infty}ig) \\ p_{\infty} = 0 \quad ext{for} \quad n_{\infty}(x,t) < 1 \\ p_{\infty}ig(\Delta p_{\infty} + G(p_{\infty})ig) = 0 \end{array} 
ight.$$

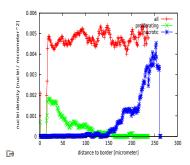
#### Remarks

- 1. Unique solution to the equation on  $n_{\infty}$  (Oleinik, Crowley)
- 2. This is a weak formulation of the geometric problem
- 3. Benilan, Caffarelli-Friedman, Gil, Quiros, Vazquez...etc









Left: The model solution

Right: Cell culture data in vitro at two different times. From N. Jagiella PhD thesis, INRIA and UPMC (2012)

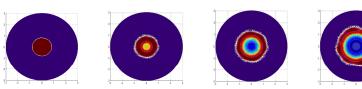


#### Model with nutrient



$$\begin{cases} \frac{\partial}{\partial t} n + \operatorname{div}(nv) = nG(p(x,t), \underbrace{c(x,t)}_{\text{nutrients}}), \\ v = -\nabla p, & p = n^{\gamma}, \\ \frac{\partial}{\partial t} c - \Delta c + \underbrace{R(n)c = c_B}_{\text{nutrients consumption/release}} \end{cases}$$

# **Open question.** $p_{\infty}(\Delta p_{\infty} + G(p_{\infty}, c_{\infty})) = 0$

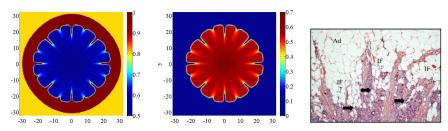




#### Model with different cells



$$\begin{cases} \frac{\partial}{\partial t} n_P + \operatorname{div}(\mu_P n_P v) = n_P G(p(x, t)) - \alpha n_P, \\ \frac{\partial}{\partial t} n_H + \operatorname{div}(\mu_H n_H v) = 0, \\ v = -\nabla p, \qquad p = (n_P + n_H)^{\gamma} \end{cases}$$



Credit for picture A. Lorz, T. Lorenzi (Saffman-Taylor instability? growth is important)

# **Concrete applications**



#### Image based predictions: include

- Active cells
- Nutrients and vasculature





■ Quiescent, necrotic, healthy cells





Credit for pictures : INRIA team Monc (Bordeaux)

# Conclusion



- 4 examples where Partial Differential Equations arise
- Many asymptotic problems
- There are concrete applications
- There are quantitative fit with experiments

■ Unlike physics, parameters are not known (distributed)

# Thanks to my co-authors



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J.-L. Vazquez, F. Quiros, A. Mellet,

A. Lorz, T. Lorenzi,



# **THANK YOU**